



resection.<sup>10</sup> The signaling molecule keratinocyte growth factor (KGF), also known as FGF7, binds to fibroblast growth factor receptor 2b (FGFR2b) and involves in the tumor growth and tissue repair with epithelial-cell specificity.<sup>11</sup> Currently, FGF7 is being used for its protective ability to epithelial cells to prevent chemoradiotherapy-associated stomatitis.<sup>12</sup> The protein kinase B, also known as Akt pathway, has been shown to be activated by FGF7. Observations have revealed that the FGF7 activation of the Akt pathway, along to its protective ability from cell apoptosis in the majority of epithelial cells, could also induce differentiation and/or cell cycle arrest in certain cell types. Therefore, it can be postulated that the balance between different signaling cascades of FGF7 leads to various and even opposite roles of this growth factor on cell growth.<sup>13,14</sup> In most normal and cancerous colonic mucosa samples, FGF7 and its receptor were detected with an overexpression of the receptor observed in the tumor cells.<sup>15</sup> According to the Human Protein Atlas (HPA) database, FGFR2b is expressed throughout the gastrointestinal tract with an overexpression in Caco-2 cells.<sup>16</sup> On the other hand, HPA has reported that no FGF7 production was detected at the protein level in Caco-2 cells.<sup>17</sup> Furthermore, it has been reported that combining mTOR and FGFR inhibitors successfully inhibited cell signaling and motility in hepatocellular carcinoma cells and impaired tumor growth in vivo.<sup>10</sup>

Virtually all cancer patients initially respond to antitumor drugs such as antiangiogenics or mTOR-inhibitors, but within few months of therapy initiation they become nonresponsive.<sup>18</sup> In the event of the treatment-targeting VEGF pathway, treatment-induced elevated tumor hypoxia often occurs, which leads to the production of a different proangiogenic mediators such as FGFs at the tumor microenvironment that lead to drug-related acquired resistance and poor prognosis.<sup>19</sup> Observations suggested that the impermeability of tumor cell membrane to most molecules diminishes the cellular uptake of anticancer drugs. Previous studies reported that no difference in EGFR-overexpressing tumor accumulation time or the biodistribution of epidermal growth factor receptor (EGFR) antibodies when compared to nontargeted therapy.<sup>20,21</sup> Thus, the difference in tumor distribution between nontargeted and targeted therapies could be evaluated by the efficient cellular uptake and retention of the drug instead of tissue-specific targeting. In this sense, the function of the targeting ligand is to prevent the potential drug clearance by tumor cells rather than to enhance the recognition at the targeted site. On that basis, several peptides and ligands-based delivery strategies of anticancer agents have been investigated.<sup>22–24</sup> These agents bind directly to a receptor overexpressed in a tumor cell and consequently improve the permeation, cellular uptake, and intracellular retention of the anticancer drug.<sup>22</sup>

In the present work, molecular-modelling tasks and in silico analysis techniques were utilized to design a new class of a potential anticancer complex to improve the efficacy of EV in CRC cells. Thereby, this study has demonstrated the in vitro cytotoxic activity of the FGF7:β-CD:EV complex on the Caco-2 cell line using real-time xCELLigence technology.

## RESULTS

**Target Identification of β-CD and EV.** Tables 1 and 2 listed the molecular targets of β-CD and EV, respectively. On the basis of the shape-similarity theory, states that the molecule-possessing similar 3D structure might exhibit an analogous biological activity. Swiss predicted with high

**Table 1. Top Five Predicted Targets of β-CD**

target	probability
fibroblast growth factor 1	0.71
fibroblast growth factor 2	0.71
vascular endothelial growth factor A	0.71
heparanase 8 kDa subunit	0.71
inactive heparanase-2	0.71

**Table 2. Top Five Predicted Targets of EV**

target	probability
serine/threonine-protein kinase mTOR	0.85
peptidyl-prolyl cis–trans isomerase FKBP1A	0.85
peptidyl-prolyl cis–trans isomerase FKBP4	0.85
peptidyl-prolyl cis–trans isomerase FKBP5	0.85
peptidyl-prolyl cis–trans isomerase FKBP1B	0.85

probability that β-CD could target FGF7 and FGF10 (also known as KGF-1 and KGF-2, respectively) based on its 3D similarity to ChEMBL198643 with a similarity score of 0.758 out of 1. It has been reported that ChEMBL198643 strongly binds with FGF1 and FGF2.<sup>25</sup> The consensus molecular targets predicted by Swiss for β-CD and EV are listed in Tables 1 and 2.

**Molecular Modeling Studies. Prediction of β-CD:EV Inclusion Complex Formation.** Molecular modeling studies for β-CD and EV interaction was performed using AutoDock Vina1.1.2. Evidence from docking scores suggested the best molecular docked conformation model of the β-CD:EV inclusion complex with a binding affinity of  $-5.31 \text{ kcal mol}^{-1}$ , which indicates good binding between β-CD (Figure 1A) and EV (Figure 1B) as well as good stability of the complex due to H-bonding (Figure 2).<sup>26,27</sup>

**Binding Ability of β-CD and EV to FGF.** Molecular docking was performed via the molecular-operating environment (MOE.2014) software for β-CD and EV in the heparin binding site of a basic fibroblast growth factor (1BFB.pdb)<sup>28</sup> with scoring affinity London dG and GBVI/WSA dG. The amino acids (Asn 28, Lys 120, Arg 121, Lys 126, Lys 136) interact with the native ligand (heparin tetramer fragment) in the binding site (Figure 3A). The docking free energy score for EV in the bind pocket of 1BFB is  $-4.4615$  (95% CI of mean =  $-4.795, -4.328$ ) with RMSD = 1.772 (95% CI of mean = 1.981, 3.682) kcal/mol. EV was able to interact with Lys 126-forming two H-bonds (Figure 3B). Additionally, β-CD was able to bind to the 1BFB binding site with a docking free energy score of  $-5.2439$  (95% CI of mean =  $-4.572, -3.740$ ) and RMSD = 1.978 (95% CI of mean = 2.174, 3.258) kcal/mol. The visualization of the interaction in the binding pocket indicated that Arg 121 formed four H-bonds with the OH groups located in different sugar rings, although Lys 126 formed a single H-bond with OH group (Figure 3C).

**FGF Binding with β-CD:EV Inclusion Complex.** The binding ability of FGF (1BFB.pdb) to the inclusion complex was assessed also using Patchdock server, clustering RMSD was set at 4.0. Simulation results have suggested that FGF tends to bind with the inclusion complex (Figure 4A) through van der Waals, electrostatic, H-bonds, and hydrophobic interactions (Figure 4B) with a binding affinity of  $-179.39 \text{ kcal mol}^{-1}$  and a binding score of 6864. Moreover, β-CD shows interaction with Ala58, Glu60, Gly 62, Arg61, Leu99, and Glu97 amino-terminal residues of FGF (Figure 4B).

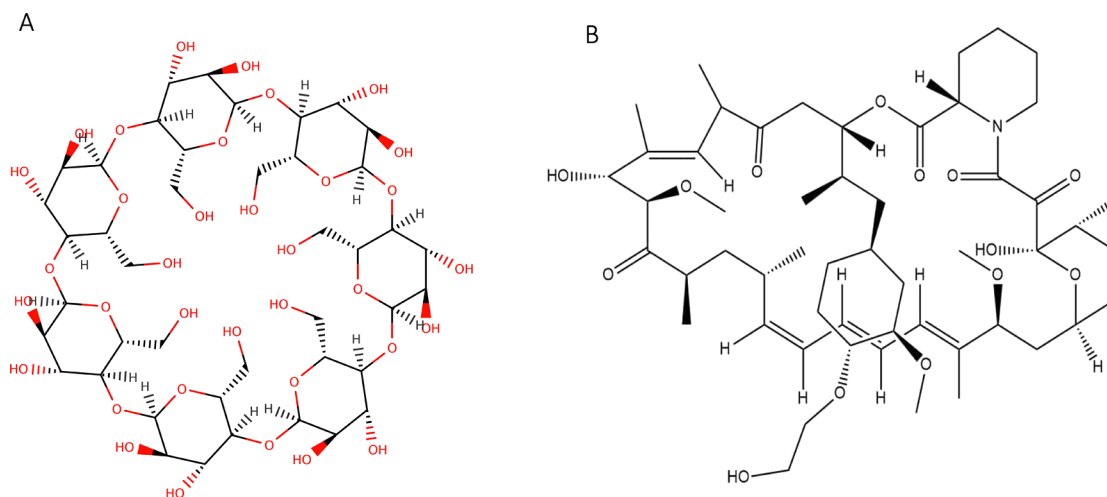


Figure 1. (A) 2D structure of  $\beta$ -CD and (B) EV.

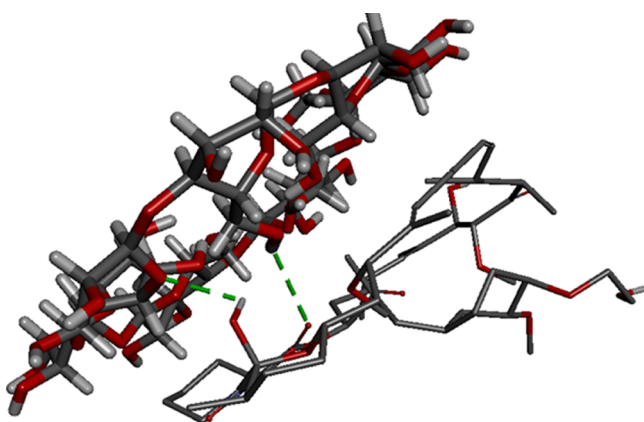


Figure 2. Best conformation model of  $\beta$ -CD:EV inclusion complex performed by Autodoc Vina 1.1.2 showing hydrogen bonds (green) interaction and binding location,  $\beta$ -CD:H142-EV:O6 with a distance of 3.05 Å and EV:H116- $\beta$ -CD:O10 with a distance of 2.57 Å.

**Preparation of Water-Soluble FGF7: $\beta$ -CD:EV Complex.** Inclusion complex of  $\beta$ -CD:EV was prepared in the 2:1 M ratio of  $\beta$ -CD and EV. The water solubility of the inclusion complex was measured by UV–Vis spectrometer and  $\lambda_{\max}$  of

the pure EV in ethanol was found to be 267 nm. The absorbance of water-soluble  $\beta$ -CD:EV complex was recorded at 280 nm, because the  $\lambda_{\max}$  shift of the UV–Vis absorption of EV was observed after the formation of the inclusion complex.<sup>29</sup> The aqueous solubility of the inclusion complex was  $3.1 \pm 0.23 \mu\text{M}$ , whereas the aqueous solubility of pure EV was  $1.7 \pm 0.16 \mu\text{M}$ . In addition, the FGF7: $\beta$ -CD:EV complex was prepared by a physical adsorption method, as a result of hydrogen bonding and hydrophobic interaction, by dissolving the FGF7 and  $\beta$ -CD:EV complex in ultra-pure water followed by freeze-drying to obtain the FGF7: $\beta$ -CD:EV complex in powder form.

**FTIR Characterization of FGF7: $\beta$ -CD:EV Complex.** The FGF7: $\beta$ -CD:EV complex was characterized by a FTIR spectrophotometer. FTIR spectrum of the complex was analyzed and compared with the spectra of the pure compounds and their physical mixture. The FTIR spectrum of EV shown characteristic peaks at  $3410 \text{ cm}^{-1}$  (OH) and  $2931 \text{ cm}^{-1}$  ( $-\text{CH}_3$ ),  $1642 \text{ cm}^{-1}$  ( $\text{C}=\text{O}$ ), and  $1448 \text{ cm}^{-1}$  ( $-\text{C}-\text{O}-\text{C}-$ ) (Figure 5A).<sup>30</sup> On the other hand, The FTIR spectrum of  $\beta$ -CD shown characteristic peaks at  $3295.22 \text{ cm}^{-1}$  (asymmetric and symmetric stretching of OH),  $2919.62 \text{ cm}^{-1}$  (asymmetric stretching from  $\text{CH}_2$ ) and  $1333 \text{ cm}^{-1}$  (coupled in plane bending of  $\text{CH}_2$ ), Figure 5B.<sup>31</sup> The physical mixture spectrum

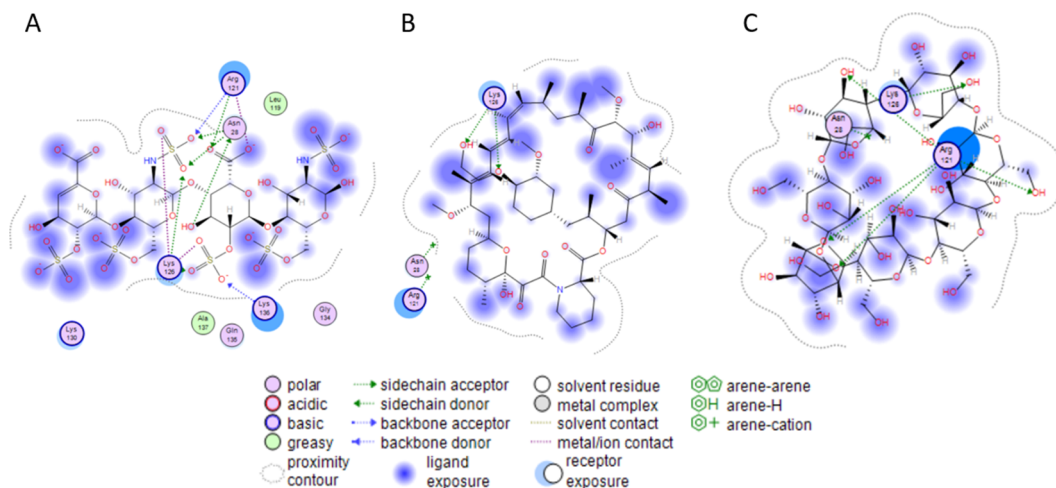
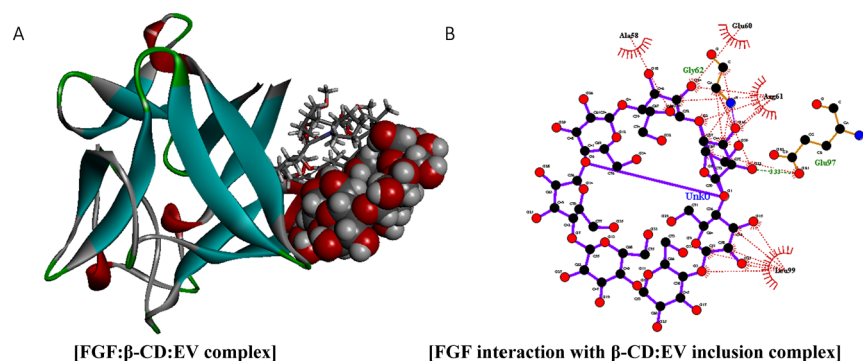
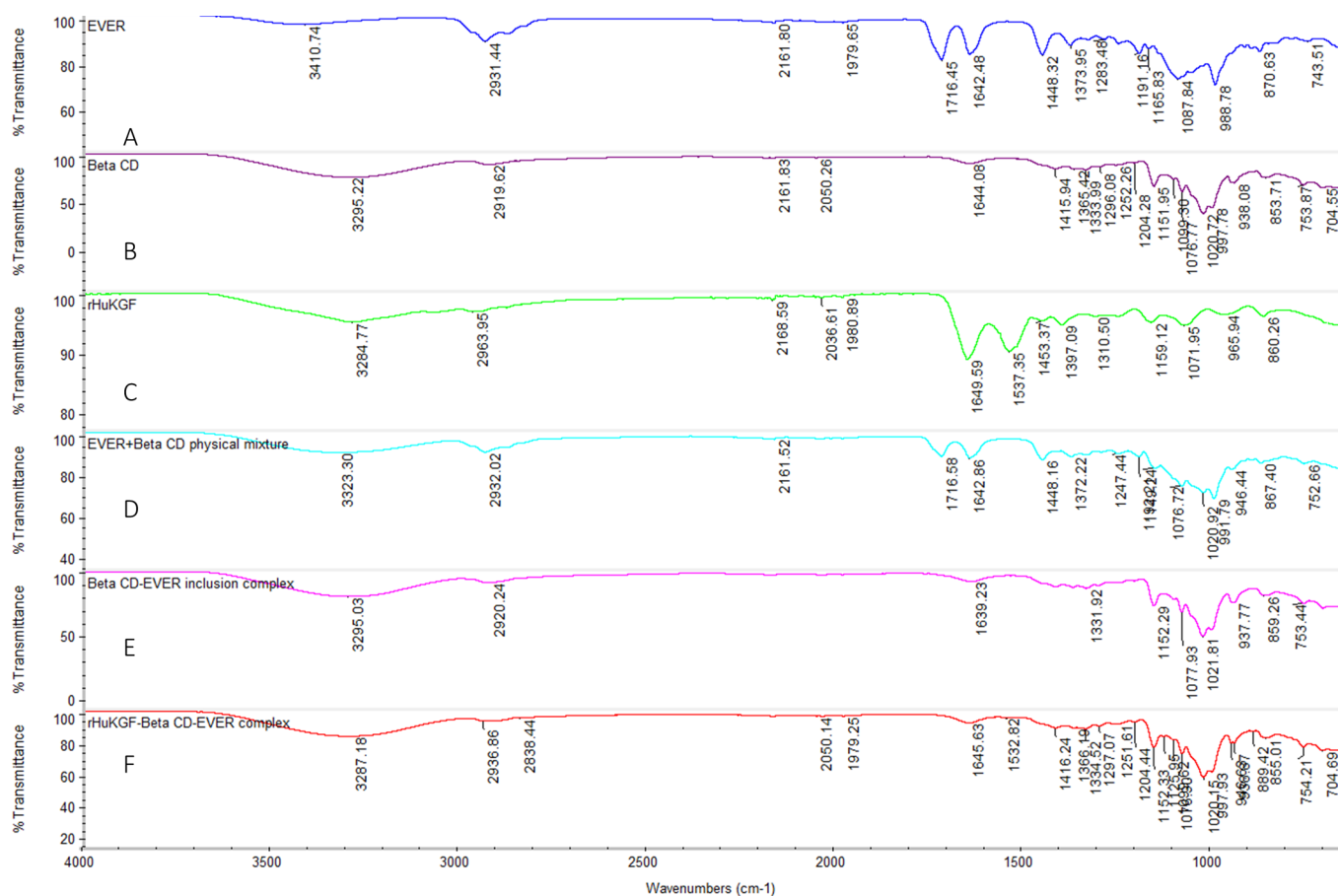


Figure 3. (A–C) 2D ligand interaction in the binding site of FGF: (A) heparin tetramer fragment, (B) EV, (C)  $\beta$ -CD.



**Figure 4.** (A) FGF (1BFb.pdb) (blue-gray stick representation) has a high binding affinity of  $-179.39$  kcal mol $^{-1}$  against  $\beta$ -CD:EV inclusion complex (red-gray ball-and-stick representation), through van der Waals, electrostatic (purple), and H-bonds (green dotted lines) interaction, (B) whereas the spoked red-arcs represent the amino-terminal residues forming hydrophobic interaction with the ligand. (C) The binding location is demonstrated with the interacting FGF amino-terminal residues.

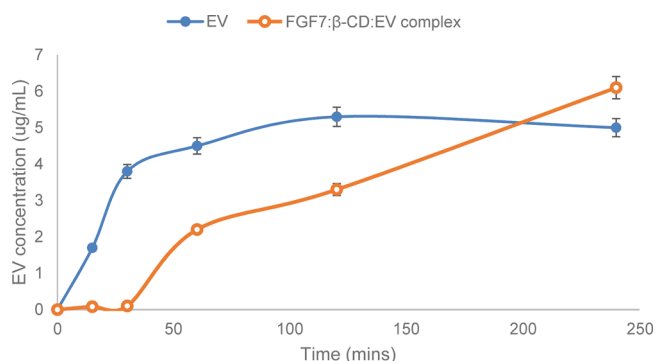


**Figure 5.** (A) FTIR spectra ( $4000$ – $1000$  cm $^{-1}$ ) of pure EV, (B)  $\beta$ -CD, (C) FGF7, (D) physical mixture of  $\beta$ -CD and EV, (E)  $\beta$ -CD:EV inclusion complex, and (F) FGF7: $\beta$ -CD:EV complex.

of EV and  $\beta$ -CD has represented all the characteristic peaks of both compounds (Figure 5D). The characteristic peaks of EV in the inclusion complex were completely vanished, indicating that the EV molecule was entirely inserted into the  $\beta$ -CD cavity (Figure 5E).<sup>32–34</sup> The FTIR spectrum of interaction of the FGF7: $\beta$ -CD:EV complex shows the characteristic peak  $1334$  cm $^{-1}$  of  $\beta$ -CD along with the characteristic peak  $1532$  cm $^{-1}$  (strong N–O stretching) of FGF7 (Figure 5F).

**Assessment of FGF7: $\beta$ -CD:EV Complex Stability and EV Release Profile.** FGF7: $\beta$ -CD:EV complex stability in Dulbecco's modified eagle medium (DMEM) culture media

and the release of EV from the complex were measured by utilizing size restricted dialysis tubing procedure (Figure S1). Figure 6 represents the release profile of EV from both the pure EV sample and FGF7: $\beta$ -CD:EV complex sample. The results revealed that after 15 min, around 27% of the pure EV sample was detected in a receiver compartment (Figure 6). On the other hand, up to 30 min of experiment, there was no detection of free EV from the FGF7: $\beta$ -CD:EV complex sample in the receiver compartment, and about 35% of free EV was detected after 1 h.



**Figure 6.** Time-dependent FGF7:β-CD:EV complex stability in DMEM culture media and the release profile of EV from the complex sample and pure EV sample ( $n = 3$ ).

**Dynamic Monitoring of Cytotoxic Activity Using RTCA DP Instrument.** To evaluate the antiproliferative efficacy of different EV complexes on Caco-2 cells, EV, FGF7:EV, β-CD:EV inclusion complex, and FGF7:β-CD:EV complex with an EV concentrations of 3.26, 6.52, and 13.04 μM were incubated with Caco-2 cells for 96 h, and the cell viability was measured by an RTCA DP instrument. Figure 7 represents the concentration-dependent cytotoxicity of EV on Caco-2 cells for over 96 h incubation time. EV exhibited an  $IC_{50}$  value of  $9.65 \pm 1.42 \mu\text{M}$  after 96 h incubation time.

The effect of exogenous FGF7 on the cytotoxicity of EV is demonstrated in Figure 8. The  $IC_{50}$  value of the FGF7:EV complex in Caco-2 cells was found to be  $3.81 \pm 0.82 \mu\text{M}$  after 96 h incubation time.

The cytotoxicity of β-CD:EV was lower than the parent drug EV, with an  $IC_{50}$  value of  $17.71 \pm 4.45 \mu\text{M}$  after 96 h incubation time (Figure 9).

Target identification software Swiss suggested that β-CD could possess a cytotoxic effect. For this reason, β-CD and β-CD-FGF were tested on Caco-2 cell line. As a result, β-CD appeared to be cytotoxic to Caco-2 cell line with  $IC_{50}$  ( $5.11 \mu\text{M}$ ). Adding β-CD and FGF together decreased the  $IC_{50}$  value to  $2.73 \mu\text{M}$ . Interestingly, the cytotoxicity of EV was remarkably improved when combined with exogenous β-CD

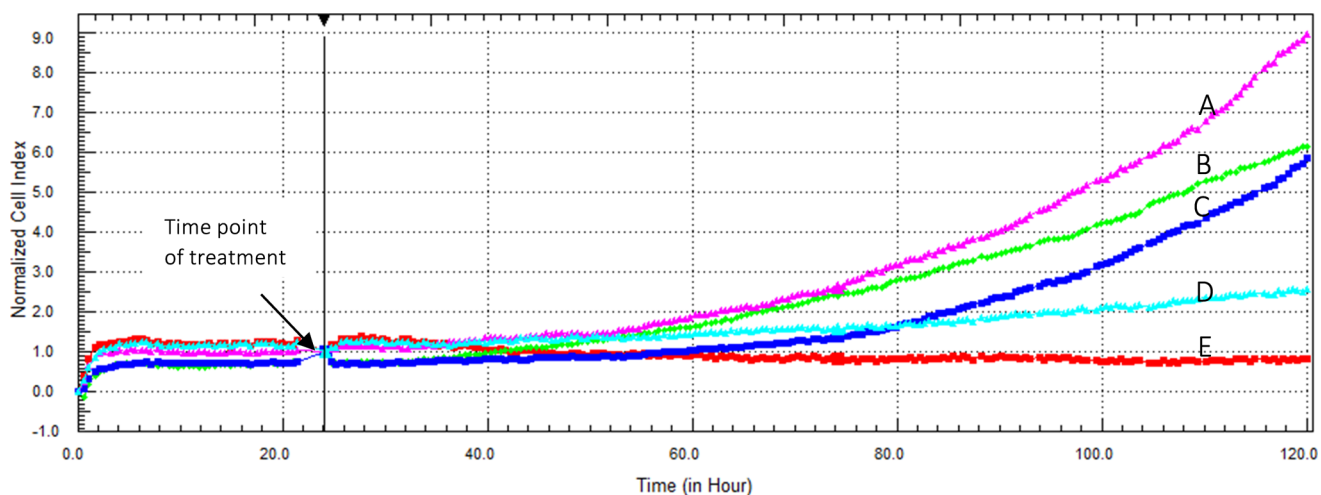
and FGF7,  $P < 0.001$  (Figure 10). Figure 11 represents the cytotoxic activity of EV for each respective complex on Caco-2 cell line after 96 h incubation time.

**Cytotoxicity of FGF7:β-CD:EV Complex on Normal Cells.** In this study, the normal human fetal small intestinal (FHs 74 Int, ATCC CCL-241) cell line was used to investigate the cytotoxicity of FGF7:β-CD:EV complex on normal human cells, and the cell viability was measured by a RTCA DP instrument. Figure S2 represents the concentration-dependent cytotoxicity of EV on FHs 74 Int cells. The Pure EV sample has exhibited an  $IC_{50}$  value of  $19.25 \pm 1.35 \mu\text{M}$  for over 72 h incubation time. The cytotoxicity of FGF7:EV and β-CD:EV complexes on FHs 74 Int cells was found to be similar to pure EV with  $IC_{50}$  values of  $15.9 \pm 0.95$  and  $16.55 \pm 1.05 \mu\text{M}$ , respectively (Figures S3 and S4). On the other hand, the cytotoxicity of the FGF7:β-CD:EV complex on FHs 74 Int cells was found to be lower ( $IC_{50} = 34.11 \pm 1.9 \mu\text{M}$ ) (Figure S5) when compare to the pure EV sample,  $P < 0.0001$ , mainly due to the fact that EV is less exposed to the cell because of its inclusion inside β-CD.

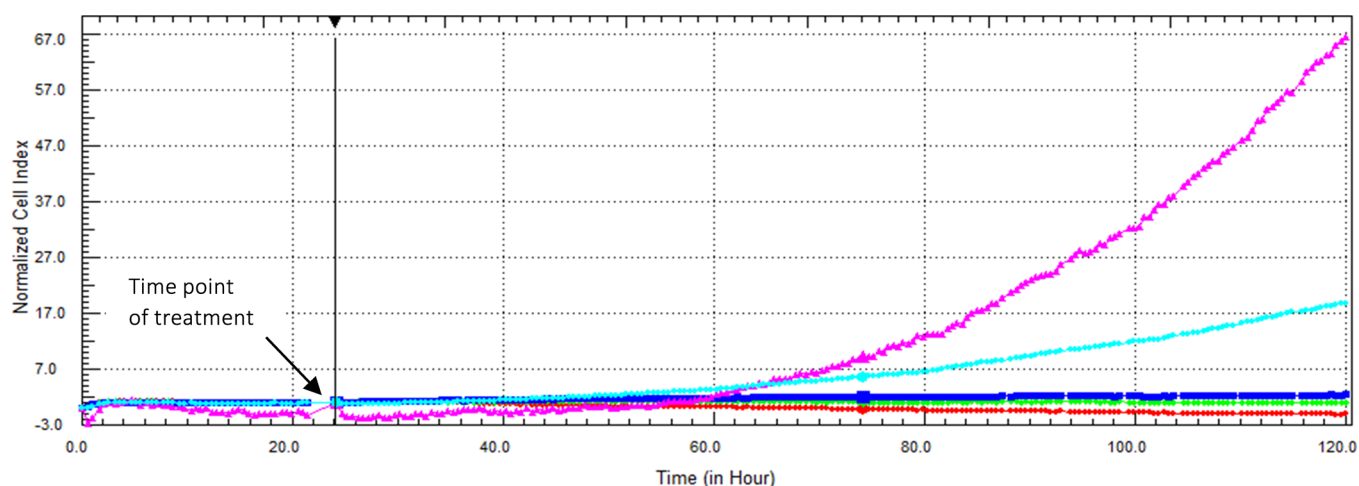
**Assessment of FGF7:β-CD:EV Complex Retention in Caco-2 Cells.** A 2D monolayer cell culture method was used to evaluate the drug uptake and retention in Caco-2 cells. The first 30 min of exposure was not considered because of the release time delay between two applications of EV to the tumor cells. The observations from Figure S6 indicated that the penetration of EV from both pure and complex samples was time-dependent, thus the intracellular accumulation of EV was significantly increased with FGF7:β-CD:EV complex application,  $P < 0.05$ , only ~2.5% of free EV from the complex sample and ~6% of the pure EV sample was detected extracellularly after 6 h. The retention of EV was enhanced with the complex application also. After 24 h of exposure, ~3.5% of free drug was detected from cells treated with the complex sample, and ~7% from cells treated with the pure EV sample.

## DISCUSSION

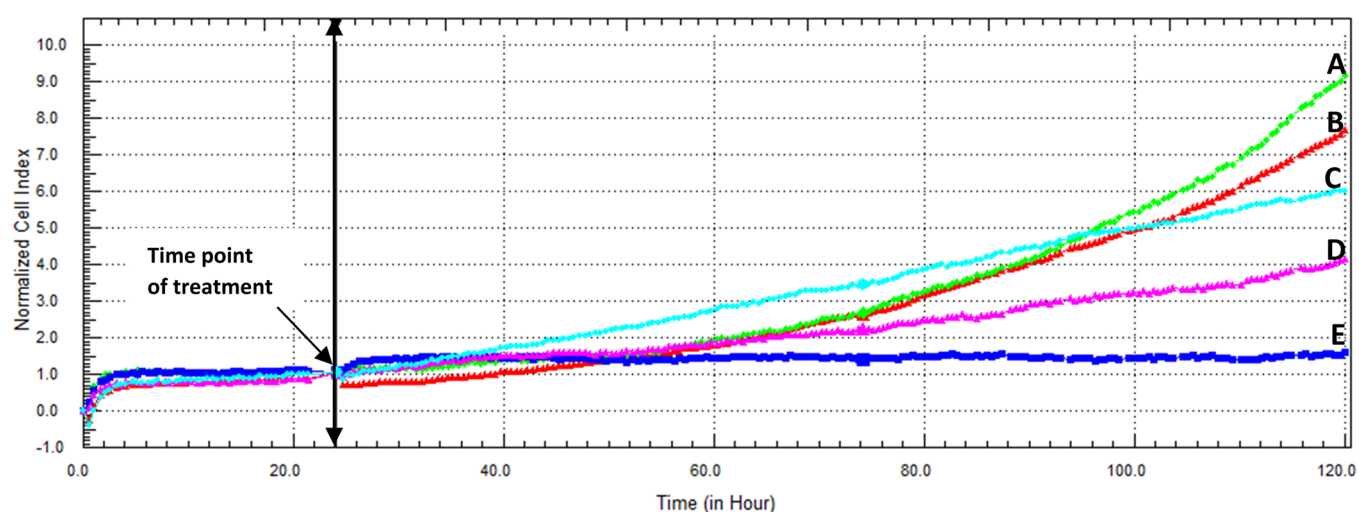
The causes of the failure of mTOR inhibitor EV as a monotherapy antitumor agent still remain unclear,<sup>35,36</sup> but several observations have linked it with cancer cell membrane



**Figure 7.** (A–E) Cytotoxic effect of EV on Caco-2 cells as displayed by the RTCA DP instrument. Cells were seeded overnight to reach the log phase, (A) then incubated with 1.58 μM FGF7, (B) media only, (C) 3.26 μM EV, (D) 6.52 μM EV, or (E) 13.04 μM EV. The  $IC_{50}$  value of EV was found to be  $9.65 \pm 1.42 \mu\text{M}$  after 96 h incubation time.



**Figure 8.** Cytotoxic effect of FGF7:EV complex on Caco-2 cells as displayed by the RTCA DP instrument. Cells were seeded overnight to reach the log phase, then incubated with 1.58  $\mu\text{M}$  FGF7 (purple), media only (light-blue), FGF7:EV complex (contains 1.58  $\mu\text{M}$  FGF7 and 3.26  $\mu\text{M}$  EV) (dark-blue), FGF7:EV (contains 1.58  $\mu\text{M}$  FGF7 and 6.52  $\mu\text{M}$  EV) (green), or FGF7:EV (contains 1.58  $\mu\text{M}$  FGF7 and 13.04  $\mu\text{M}$  EV) (red). The  $\text{IC}_{50}$  value of the FGF7:EV complex was found to be  $3.81 \pm 0.82 \mu\text{M}$  after 96 h incubation time.

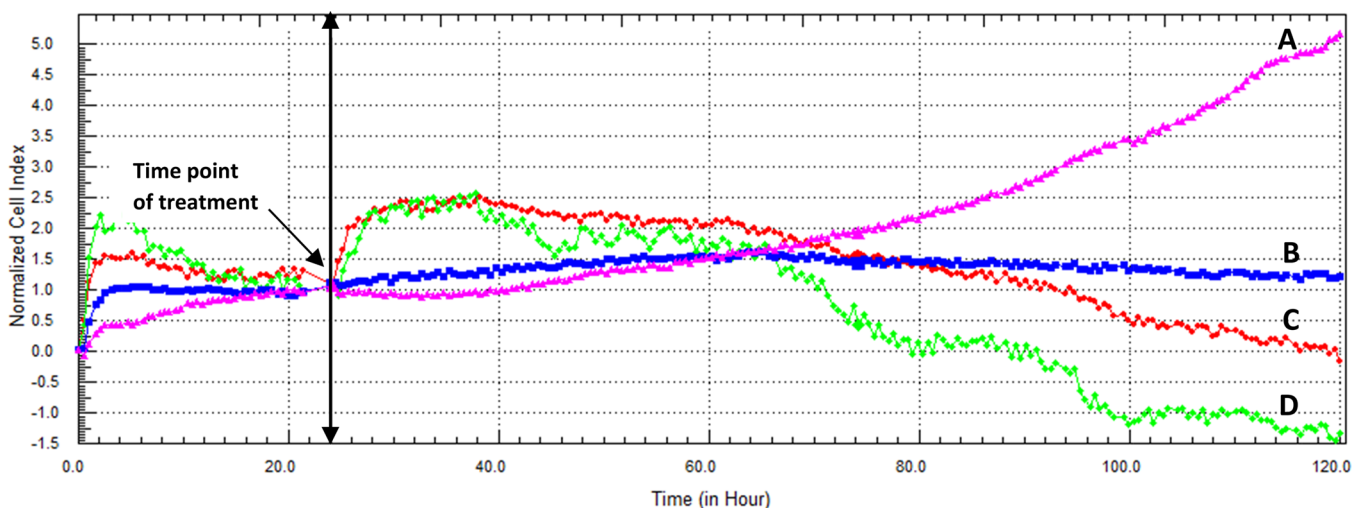


**Figure 9.** (A–E) Cytotoxic effect of  $\beta\text{-CD:EV}$  inclusion complex on Caco-2 cells as displayed by the RTCA DP instrument. (A) Cells were seeded overnight to reach the log phase, then incubated with media only, (B)  $\beta\text{-CD}$  only, (C)  $\beta\text{-CD:EV}$  inclusion complex (contains 3.26  $\mu\text{M}$  EV), (D)  $\beta\text{-CD:EV}$  inclusion complex (contains 6.52  $\mu\text{M}$  EV), or (E)  $\beta\text{-CD:EV}$  inclusion complex (contains 13.04  $\mu\text{M}$  EV). The  $\text{IC}_{50}$  value of  $\beta\text{-CD:EV}$  inclusion complex was found to be  $17.71 \pm 4.45 \mu\text{M}$  after 96 h incubation time.

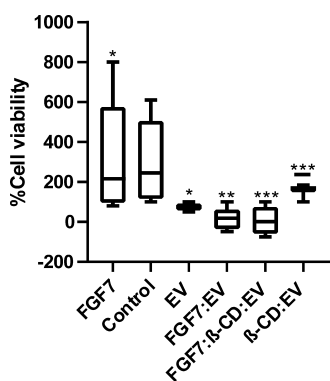
barriers, P-gp active efflux transporter or multidrug resistance-associated proteins.<sup>37</sup>  $\beta\text{-CD}$  has been reported to increase the retention and accumulation of mTOR inhibitors in Caco-2 cells by significant decrease in the efflux ratio, suggesting the inhibition of P-gp-mediated efflux transport.<sup>38–40</sup> Besides, increasing the retentions of mTOR inhibitors, we want to identify the molecular targets of  $\beta\text{-CD}$ . A Swiss target identification analysis was used to identify  $\beta\text{-CD}$  molecular targets. Swiss suggested that  $\beta\text{-CD}$  is capable to bind to FGF1 and FGF2. This could be supported by the strong affinity of a similar structure ( $\beta\text{-CD}$  tetradecasulfate) toward FGF.<sup>41</sup> Heparin is essential for FGF to generate a biological response by binding to a FGF receptor. Heparin functions by binding to several FGF molecules forming FGF oligomerization. Then the FGF-heparin complex bind to couple of FGFRs, this leads to FGFR dimerization, which activates tyrosine kinase pathway (Figure 12A). A study showed that synthetic heparin analog, which can only bind to one FGF, blocks the dimerization of FGFR, thus stop its activation. We propose that  $\beta\text{-CD}$

antagonizes the action of heparin by binding to only one FGF; therefore, it cannot induce FGF oligomerization thus preventing FGFR dimerization.<sup>42,43</sup> This prevent FGFR activation and suppresses the intracellular cascades of FGFR, leading to cell growth inhibition (Figure 12B).

In the current work, the influence of exogenous FGF7 and  $\beta\text{-CD}$  on the cytotoxic activity of the parent drug EV was investigated in Caco-2 cell line. Molecular modeling studies were performed to predict the binding affinity of the FGF: $\beta\text{-CD:EV}$  complex. First as shown in Figure 2, Ligand–ligand docking was performed using Autodock vina. An EV molecule was successfully docked into  $\beta\text{-CD}$  cavity with a binding affinity of  $-5.3 \text{ kcal mol}^{-1}$ . Because hydroxyl groups surround the narrow opening of  $\beta\text{-CD}$ , EV binding with this narrow opening of  $\beta\text{-CD}$  indicates possibility of H-bonding between EV oxygen atoms and hydroxyl groups of  $\beta\text{-CD}$  near the narrow opening. In addition, MOE was used to dock  $\beta\text{-CD}$  and EV (individually) in the heparin binding site of FGF (IBFB) with docking free energy score of  $-5.2439$  and  $-4.4615$ ,



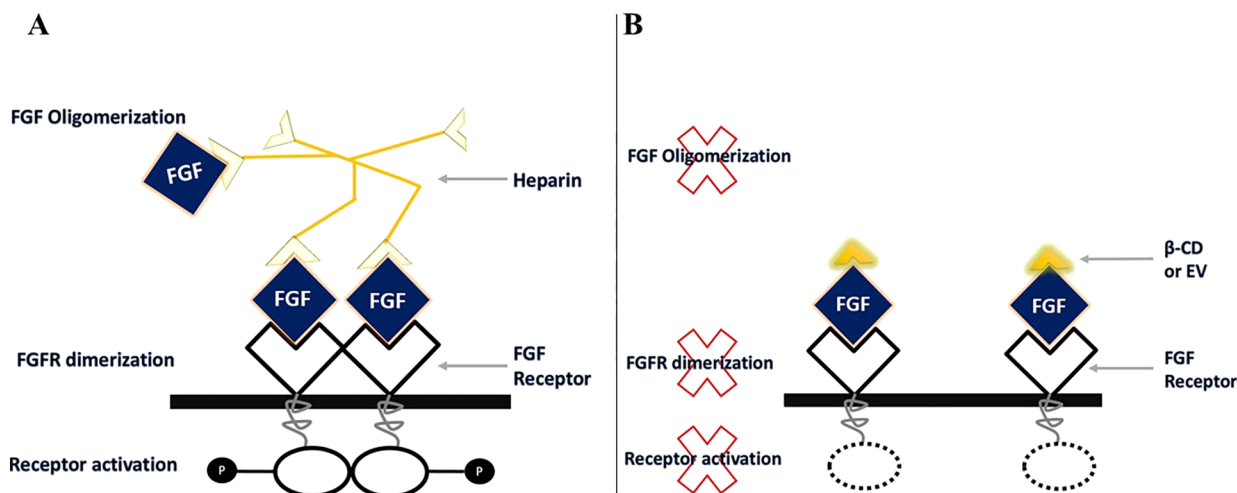
**Figure 10.** (A–D) Cytotoxic effect of FGF7: $\beta$ -CD:EV complex on Caco-2 cells as displayed by the RTCA DP instrument. (A) Cells were seeded overnight to reach the log phase, then incubated with media only. (B) FGF7: $\beta$ -CD:EV complex (contains 1.58  $\mu$ M FGF7 and 3.26  $\mu$ M EV). (C) FGF7: $\beta$ -CD:EV complex (contains 1.58  $\mu$ M FGF7 and 6.52  $\mu$ M EV). (D) FGF7: $\beta$ -CD:EV complex (contains 1.58  $\mu$ M FGF7 and 13.04  $\mu$ M EV). The  $IC_{50}$  value of FGF7: $\beta$ -CD:EV complex was found to be  $1.87 \pm 0.33 \mu$ M after 96 h incubation time.



**Figure 11.** In vitro activity determination of EV, FGF7:EV,  $\beta$ -CD:EV, and FGF7: $\beta$ -CD:EV complexes. Results have demonstrated the cell growth by EV as the percentage of the control determined using RTCA xCELLigence technology after 96 h incubation time in Caco-2 cell lines ( $n = 6$ ). In general, a 100% cell kill is only observed with the FGF7: $\beta$ -CD:EV complex and FGF7:EV complex. \* $P < 0.05$ , \*\* $P < 0.01$ . \*\*\* $P < 0.001$ .

respectively (Figure 3). FGF has shown a binding affinity of  $-179.39 \text{ kcal mol}^{-1}$  to the  $\beta$ -CD:EV inclusion complex through van der Waals, electrostatic, H-bonds, and hydrophobic interactions (Figure 4), suggested a good stability of FGF: $\beta$ -CD:EV complex.

In this study,  $\beta$ -CD was utilized to enhance the aqueous solubility of EV. Hence, the therapeutic application of the majority of anticancer drugs is severely limited because of their poor water-solubility and inadequate cancer cell penetration.<sup>44,45</sup>  $\beta$ -CD is capable to form a stable inclusion complex with EV at molecular level based on hydrophobic interactions as the EV molecule inserts into the  $\beta$ -CD cavity.<sup>45,46</sup> The aqueous solubility of the inclusion complex was increased by ( $3.1 \pm 0.23 \mu$ M) when compared to the aqueous solubility of pure EV ( $1.7 \pm 0.16 \mu$ M). FTIR studies indicate that a new structure was formed, and the EV molecule was entirely embedded into the  $\beta$ -CD cavity (Figure 5E) as the characteristic peaks of EV were completely vanished.<sup>32–34</sup> Furthermore, the interaction of FGF7 with the  $\beta$ -CD:EV inclusion complex was determined also. There was a shifting of



**Figure 12.** (A) Heparin induced FGF oligomerization and activate FGFR. (B)  $\beta$ -CD or EV binds to only one FGF preventing FGFR dimerization.

the broad classic band of  $\beta$ -CD from 3295.22 to 3287  $\text{cm}^{-1}$ , indicating a possibility of H-bonding between FGF7 and the inclusion complex as suggested by the molecular modeling scores (Figure 4). The FGF7: $\beta$ -CD:EV complex stability in a DMEM media and the release of EV were measured by dialysis tubing procedure (Figure S1). Up to 30 min of experiment, there was no detection of free EV from the FGF7: $\beta$ -CD:EV complex sample in a receiver compartment, and about 35% of free EV was detected after 1 h time. This indicated that the complex is stable in DMEM for at least 30 min and exhibits sustain release profile (up to 4 h).

RTCA xCELLigence technology results revealed that when cells are treated with EV alone, the  $\text{IC}_{50}$  value was  $9.65 \pm 1.42 \mu\text{M}$ . Treating cells with FGF and EV resulted in increase in the cytotoxicity significantly with  $\text{IC}_{50}$  ( $3.81 \pm 0.82 \mu\text{M}$ ) ( $P < 0.05$ ) compare to EV alone. Considering the molecular docking result, we believe that part of the EV molecules binds to FGF and inhibiting FGF oligomerization, whereas the rest goes inside the cells and act as mTOR inhibitor. This can be supported by  $\beta$ -CD and  $\beta$ -CD:FGF cytotoxicity results. In our view when cells are treated with  $\beta$ -CD alone ( $\text{IC}_{50} = 5.11 \mu\text{M}$ ),  $\beta$ -CD tries to substitute heparin from the existing FGF in the cells preventing FGF oligomerization; however, by adding both  $\beta$ -CD and FGF together, they decreased the  $\text{IC}_{50}$  value to  $2.73 \mu\text{M}$  by directly working as a complex to block FGFR, preventing more receptors to be activated. The  $\text{IC}_{50}$  value of  $\beta$ -CD:EV was higher than that of EV, suggesting that conjugation significantly affect EV efficacy ( $P < 0.01$ ), possibly due to the slow release profile of EV from the inclusion complex.<sup>47,48</sup> Interestingly, the cytotoxicity of the  $\beta$ -CD:EV inclusion complex was remarkably improved when combined with FGF7,  $P < 0.001$  (Figure 10) with a dramatic decrease in the  $\text{IC}_{50}$  value from  $17.71 \pm 1.42$  to  $1.87 \pm 0.33 \mu\text{M}$ . Hence, FGF7 facilitated the intracellular delivery of EV. Also, according to the molecular docking result, both EV and  $\beta$ -CD are capable to bind in the heparin binding site of FGF; however,  $\beta$ -CD has a higher binding score and has more hydrogen bonds compare to EV. We assume that in the presence of the  $\beta$ -CD and FGF, most of EV molecules are able to enter the cells and act as an mTOR inhibitor, whereas  $\beta$ -CD binds to FGF and inhibits its oligomerization. Therefore, the multitargets effect of the complex facilitating the cellular uptake of EV, preventing FGF receptors activation, and enhancing the intracellular retention of EV. The antiproliferative effect of EV in Caco-2 cells was remarkably improved as the least  $\text{IC}_{50}$  value was obtained with the FGF7: $\beta$ -CD:EV complex. Lastly, the concentration-dependent cytotoxicity of pure EV and FGF7: $\beta$ -CD:EV complex on FHs 74 Int normal cell line was studied. A pure EV sample exhibited an  $\text{IC}_{50}$  value of  $19.25 \pm 1.35 \mu\text{M}$  at over 72 h incubation time. The cytotoxicity of the FGF7: $\beta$ -CD:EV complex on FHs 74 Int cells was found to be lower ( $\text{IC}_{50} = 34.11 \pm 1.9 \mu\text{M}$ ) when compare to the pure EV sample,  $P < 0.0001$ , mainly due to the fact that EV is less exposed to the cell because of its inclusion inside  $\beta$ -CD.

## CONCLUSIONS

Molecular modeling tasks and in silico analysis techniques were utilized to design a new class of a potential anticancer complex to improve the efficacy of EV in the Caco-2 cell line. This study demonstrated that a FGF7: $\beta$ -CD complex dramatically improved the antiproliferative effect of the mTOR inhibitor EV by enhancing its cellular uptake,

intracellular retention, and through preventing FGFR activation thus preventing cell proliferation and possessed less toxicity in the FHs 74 Int normal human cell line. These findings advance the understanding of the biological combinational effects of the  $\beta$ -CD:FGF7 complex and EV as an effective therapeutic to combat CRC.

## MATERIALS AND METHODS

**Cell Culture and Reagents.** Caco-2 HTB-37 (ATCC, USA), FHs 74 Int (ATCC, USA), streptomycin/penicillin solution (Gibco, USA), phosphate-buffered saline (PBS) (Gibco, USA), and trypsin/EDTA (Gibco, USA),  $\beta$ -Cyclodextrin (Sigma Aldrich, USA), Dulbecco's modified eagle medium (ATCC, USA), fetal bovine serum (Gibco, USA), and EV (Toronto Research Chemicals, Canada).

**Target Identification of  $\beta$ -CD and EV.** Swiss predicts the molecular targets of small molecules based on their 2D and 3D similarity by comparing the query molecule to a library of 280 thousand compounds. SMILES of  $\beta$ -CD and EV were obtained from PubChem and were entered into Swiss target software to predict the molecular targets of  $\beta$ -CD and EV.<sup>49</sup>

**Molecular Modeling Studies.** Molecular modeling studies were performed to predict the formation of  $\beta$ -CD:EV, FGF7: $\beta$ -CD, and FGF7:EV complexes and to measure their binding affinity by utilizing AutoDock Vina 1.1.2,<sup>50</sup> PatchDock server,<sup>51,52</sup> and MOE.2014 software, which are available from the Chemical Computing Group (CCG; [www.chemcomp.com](http://www.chemcomp.com)). The 3D structures of EV (PubChem CID: 6442177)<sup>53</sup> and  $\beta$ -CD (PubChem CID: 444041)<sup>54</sup> were obtained from NCBI PubChem compound database where the structural complex of FGF7 (PDB ID: 1BFB)<sup>28</sup> was retrieved from RCSB Protein Data Bank (PDB). All structures of the selected compounds, served as molecules for modeling studies, were optimized through MOE.2014 software before docking. Hydrogen atoms and partial charges were added to the protein. Protein minimization was performed in gas solvation with the side chains, keeping it rigid and the ligand flexible.<sup>55</sup> The selected site was isolated and minimized, followed by protonating the protein. The 3D ligands were minimized using MMFF94x with cutoffs of 10 to 12 Å. The hydrogens and charges were fixed, and the RMS gradient was set to 0.001 kcal/mol.<sup>56</sup> To perform docking with AutoDock Vina software v1.1.2, the receptor and ligand structures were transformed to the PDBQT file format, which included atomic charges, atom-type definitions, and for the ligands as well as the topological information (rotatable bonds). A grid with dimensions of  $23 \times 23 \times 23$  points was centered to the co-crystallized ligands to ensure the coverage of the binding site of the structure. Default parameter PatchDock server was set as clustering root mean square deviation (RMSD) at 4.0 and docked poses were analyzed by LigPlot Plus for generating 2D schematic representations.<sup>57,58</sup>

**Preparation of Water-Soluble FGF7: $\beta$ -CD:EV Complex.** The  $\beta$ -CD:EV inclusion complex was prepared in a 2:1 M ratio. Briefly, 10 mg of EV and 20 mg of  $\beta$ -CD were completely dissolved in (1:1 v/v) mixture of ethanol and 30% ammonium hydroxide. The solution was filtered through a  $0.45 \mu$  membrane filter, and the filtrate was evaporated under reduced pressure and dried in a vacuum oven.<sup>59,60</sup> The water solubility of the inclusion complex was measured by double-beam UV-Vis spectrometer (PerkinElmer, USA). Briefly, a five-point calibration curve of EV was prepared in ethanol and absorbance was recorded at 267 nm,  $\lambda_{\text{max}}$  ( $n = 6$ ).



Furthermore, a known amount of inclusion complex powder was dissolved in distilled water, the absorbance was recorded at 280 nm,  $\lambda_{\max}$  of the inclusion complex, and EV concentration was determined ( $n = 6$ ) accordingly. Furthermore, the FGF7: $\beta$ -CD:EV complex was prepared by a physical adsorption method by dissolving 6  $\mu$ g FGF7 and  $\beta$ -CD:EV complex in ultra-pure water followed by freeze-drying for over 24 h (at  $-34$  °C and gradual ascent up to 20 °C), using a Labconco freeze dryer (Labconco, USA) to obtain the FGF7: $\beta$ -CD:EV complex in a powder form.

**FTIR Characterization of FGF7- $\beta$ -CD-EV Complex.** For the physical mixture of FGF7,  $\beta$ -CD, and EV, the FGF7: $\beta$ -CD:EV inclusion complex were characterized by FTIR. All spectra were obtained by a Thermo Fisher Scientific Nicolet iS5 spectrophotometer (Wisconsin, USA) using OMNIC software from 1000 to 4000  $\text{cm}^{-1}$  at a data acquisition rate of 2  $\text{cm}^{-1}$  per point.

**Assessment of FGF7: $\beta$ -CD:EV Complex Stability and EV Release Profile in DMEM.** A size-restricted dialysis tubing procedure was employed to measure the FGF7: $\beta$ -CD:EV complex stability in a culture media and the release of EV from the complex. Briefly, complex stability and EV release from known amounts of complex (contains 6.52  $\mu$ M of EV) were determined using a modified dissolution method. The medium comprised of a 0.05 M phosphate buffer solution (PBS) pH 7.4. The dialysis bags (MWCO 2000 Da, Sigma, Germany) were filled with known amount of complex along with cell culture media and placed in 50 mL PBS (pH 7.4) at 37 °C with slow magnetic stirring (50 rpm) under perfect sink conditions. One mL of aliquots was withdrawn from the external solution and replaced with the same volume of fresh PBS. The drug concentration was detected by HPLC (Flexar FX-20, PerkinElmer, USA) at 278 nm. All experiments were carried out in triplicate and performed as at least three independent experiments.

**Cell Culture.** Caco-2 (ATCC HTB-37) and FHs 74 Int (ATCC CCL-241) cells were maintained in ATCC-formulated DMEM supplemented with 10% fetal bovine serum, 1% penicillin/streptomycin, and cells were incubated under a humidified atmosphere of 5%  $\text{CO}_2$  and 95% air at 37 °C.

**Dynamic Monitoring of Cytotoxic Activity Using RTCA DP System.** Real-time cellular analysis (RTCA) xCELLigence technology was used for screening of cytotoxicity by monitoring the cellular events in real-time during the entire time course of the experiment and to obtain more reveals about when and the rate of cellular responses.<sup>61</sup> Caco-2 cells were seeded in E-plates 16 at a concentration of  $5 \times 10^3$ , grown overnight to reach the log phase, then treated with EV, FGF7:EV,  $\beta$ -CD:EV, and FGF7: $\beta$ -CD:EV complexes (each complex contained 3.26, 6.52, and 13.04  $\mu$ M EV) or medium alone, and cell responses were monitored by taking xCELLigence RTCA DP instrument (ACEA Biosciences Inc., USA) readings every 5 min for 24 h and every 30 min for 96 h. The kinetic profile of the cellular responses, the decrease in cell index, and  $\text{IC}_{50}$  values as per each complex were obtained accordingly against their respective concentrations.<sup>62</sup>

**Assessment of FGF7: $\beta$ -CD:EV Complex Retention in Caco-2 Cells.** Two-dimensional (2D) monolayer cell culture models are the most common method used to investigate tumor cells in vitro.<sup>63</sup> We used a 2D monolayer cell culture system to identify the rate of EV penetration and the extent of drug accumulation in cancer cells. The experimental model

used was the human colorectal cancer Caco-2 cells. Drug accumulation was determined by the extracellular concentration gradient of free EV and the relationship between exposure time and drug accumulation was investigated.<sup>64</sup> Briefly, cells were seeded in 6-well plate at a concentration of  $5 \times 10^4$  per well and allowed to grow for 24 h. Cells were incubated at 37 °C with the FGF7: $\beta$ -CD:EV complex and EV only, each contain 6.52  $\mu$ M EV, and the extracellular concentration of the free EV was measured at different time intervals by HPLC (PerkinElmer, USA) (for chromatographic conditions see the Supporting Information). All experiments were carried out in triplicate and performed as at least three independent experiments.

**Statistical Analysis.** The results are expressed as mean  $\pm$  standard deviation (SD) ( $n = 6$ ), and the statistical analysis was performed with GraphPad Prism 8 (GraphPad Software, Inc., La Jolla, CA, USA). The significance of any differences between experimental groups was evaluated by the one-way ANOVA followed by a Turkey–Kramer multiple comparisons test. The calculation of  $\text{IC}_{50}$  values of EV as per each complex was obtained using xCELLigence RTCA DP software.  $\text{IC}_{50}$  values were expressed as the mean (M)  $\pm$  S.E.M. ( $n = 6$ ). The 95% confidence intervals (CIs) of the binding affinity (according to their mean and standard errors) were estimated with 2.5 and 97.5 percentile as the lower and upper bounds. Error bars represent the standard error of the mean.

## ■ ASSOCIATED CONTENT

### 📄 Supporting Information

The Supporting Information is available free of charge on the ACS Publications website at DOI: 10.1021/acsomega.9b00109.

Diagram of dialysis tubing procedure, raw data of cytotoxicity on FHs 74 Int cells, HPLC chromatographic conditions, raw data of complex retention in Caco-2 cells, standard chromatogram of EV, raw data of Swiss target prediction, and docking scores for binding affinity of  $\beta$ -CD and EV to FGF7 (PDF)

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### Notes

The authors declare no competing financial interest.

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## ■ REFERENCES

(1) Su, Y.-C.; Liao, H.-F.; Yu, C.-C.; Lin, Y.-C. Anticancer activity of the mTOR inhibitor (everolimus) and dual mTORC1/mTORC2 Inhibitor (AZD2014) on mouse lymphocytic leukemia both in vitro and in vivo. *Ann. Oncol.* **2016**, *27*, 29.

- (2) Vijayaraj Kumar, P.; Venkata Subramanya Lokesh, B. Designing and In-Vitro Characterization of Micelle Forming Amphiphilic PEGylated Rapamycin Nanocarriers for the Treatment of Gastric Cancer. *Curr. Drug Delivery* **2014**, *11*, 613–620.
- (3) Pavel, M. E.; Hainsworth, J. D.; Baudin, E.; Peeters, M.; Hörsch, D.; Winkler, R. E.; Klimovsky, J.; Lebwohl, D.; Jehl, V.; Wolin, E. M.; Öberg, K.; Van Cutsem, E.; Yao, J. C. Everolimus plus octreotide long-acting repeatable for the treatment of advanced neuroendocrine tumours associated with carcinoid syndrome (RADIANT-2): a randomised, placebo-controlled, phase 3 study. *Lancet* **2011**, *378*, 2005–2012.
- (4) Ng, K.; Taberero, J.; Hwang, J.; Bajetta, E.; Sharma, S.; Del Prete, S. A.; Arrowsmith, E. R.; et al. Phase II study of everolimus in patients with metastatic colorectal adenocarcinoma previously treated with bevacizumab-, fluoropyrimidine-, oxaliplatin-, and irinotecan-based regimens. *Clin. Cancer Res.* **2013**, *27*, 3987.
- (5) Spindler, K.-L. G.; Sorensen, M. M.; Pallisgaard, N.; Andersen, R. F.; Havelund, B. M.; Ploen, J.; Lassen, U.; Jakobsen, A. K. M. Phase II trial of temsirolimus alone and in combination with irinotecan for KRAS mutant metastatic colorectal cancer: outcome and results of KRAS mutational analysis in plasma. *Acta Oncol.* **2013**, *52*, 963–970.
- (6) Castellano, D.; Bajetta, E.; Panneerselvam, A.; Saletan, S.; Kocha, W.; O'Dorisio, T.; Anthony, L. B.; Hobday, T. Everolimus plus octreotide long-acting repeatable in patients with colorectal neuroendocrine tumors: a subgroup analysis of the phase III RADIANT-2 study. *Oncologist* **2013**, *18*, 46–53.
- (7) Wang, X.-W.; Zhang, Y.-J. Targeting mTOR network in colorectal cancer therapy. *World J. Gastroenterol.* **2014**, *20*, 4178.
- (8) Gullotti, E.; Yeo, Y. Extracellularly Activated Nanocarriers: A New Paradigm of Tumor Targeted Drug Delivery. *Mol. Pharmaceutics* **2009**, *6*, 1041–1051.
- (9) Mousa, L.; Salem, M. E.; Mikhail, S. Biomarkers of Angiogenesis in Colorectal Cancer: Supplementary Issue: Biomarkers for Colon Cancer. *Biomarkers in Cancer* **2015**, *7*, 13.
- (10) Scheller, T.; Hellerbrand, C.; Moser, C.; Schmidt, K.; Kroemer, A.; Brunner, S. M.; Schlitt, H. J.; Geissler, E. K.; Lang, S. A. mTOR inhibition improves fibroblast growth factor receptor targeting in hepatocellular carcinoma. *Br. J. Cancer* **2015**, *112*, 841.
- (11) Rubin, J. S.; Bottaro, D. P.; Chedid, M.; Miki, T.; Ron, D.; Cunha, G. R.; Finch, P. W. Keratinocyte growth factor as a cytokine that mediates mesenchymal-epithelial interaction. In *Epithelial-Mesenchymal Interactions in Cancer*; Springer: 1995; pp 191–214.
- (12) D'Hondt, L.; Lonchay, C.; André, M.; Cannon, J.-L. Oral mucositis induced by anticancer treatments: physiopathology and treatments. *Ther. Clin. Risk Manage.* **2006**, *2*, 159.
- (13) Calautti, E.; Li, J.; Saoncella, S.; Brissette, J. L.; Goetinck, P. F. Phosphoinositide 3-kinase signaling to Akt promotes keratinocyte differentiation versus death. *J. Biol. Chem.* **2005**, *280*, 32856–32865.
- (14) Lotti, L. V.; Rotolo, S.; Francescangeli, F.; Frati, L.; Torrisi, M. R.; Marchese, C. AKT and MAPK signaling in KGF-treated and UVB-exposed human epidermal cells. *J. Cell. Physiol.* **2007**, *212*, 633–642.
- (15) Otte, J. M.; Schmitz, F.; Banasiewicz, T.; Drews, M.; Fölsch, U. R.; Herzig, K. H. Expression of keratinocyte growth factor and its receptor in colorectal cancer. *Eur. J. Clin. Invest.* **2000**, *30*, 222–9.
- (16) *Fibroblast growth factor receptor 2*. <https://www.proteinatlas.org/ENSG00000066468-FGFR2/cell>.
- (17) *Fibroblast growth factor 7*. <https://www.proteinatlas.org/ENSG00000140285-FGF7/cell>.
- (18) Kerbel, R. S. Tumor angiogenesis. *N. Engl. J. Med.* **2008**, *358*, 2039–2049.
- (19) Casanovas, O.; Hicklin, D. J.; Bergers, G.; Hanahan, D. Drug resistance by evasion of antiangiogenic targeting of VEGF signaling in late-stage pancreatic islet tumors. *Cancer Cell* **2005**, *8*, 299–309.
- (20) Mamot, C.; Drummond, D. C.; Noble, C. O.; Kallab, V.; Guo, Z.; Hong, K.; Kirpotin, D. B.; Park, J. W. Epidermal growth factor receptor-targeted immunoliposomes significantly enhance the efficacy of multiple anticancer drugs in vivo. *Cancer Res.* **2005**, *65*, 11631–11638.
- (21) Kirpotin, D. B.; Drummond, D. C.; Shao, Y.; Shalaby, M. R.; Hong, K.; Nielsen, U. B.; Marks, J. D.; Benz, C. C.; Park, J. W. Antibody targeting of long-circulating lipidic nanoparticles does not increase tumor localization but does increase internalization in animal models. *Cancer Res.* **2006**, *66*, 6732–6740.
- (22) Lin, C.; Zhang, X.; Chen, H.; Bian, Z.; Zhang, G.; Riaz, M. K.; Tyagi, D.; Lin, G.; Zhang, Y.; Wang, J.; Lu, A.; Yang, Z. Dual-ligand modified liposomes provide effective local targeted delivery of lung-cancer drug by antibody and tumor lineage-homing cell-penetrating peptide. *Drug Delivery* **2018**, *25*, 256–266.
- (23) Borrelli, A.; Tornesello, A. L.; Tornesello, M. L.; Buonaguro, F. M. Cell penetrating peptides as molecular carriers for anti-cancer agents. *Molecules* **2018**, *23*, 295.
- (24) Trabulo, S.; Cardoso, A. L.; Mano, M.; De Lima, M. C. P. Cell-penetrating peptides—mechanisms of cellular uptake and generation of delivery systems. *Pharmaceutics* **2010**, *3*, 961–993.
- (25) Karoli, T.; Liu, L.; Fairweather, J. K.; Hammond, E.; Li, C. P.; Cochran, S.; Bergefall, K.; Trybala, E.; Addison, R. S.; Ferro, V. Synthesis, biological activity, and preliminary pharmacokinetic evaluation of analogues of a phosphosulfomannan angiogenesis inhibitor (PI-88). *J. Med. Chem.* **2005**, *48*, 8229–8236.
- (26) Du, X.; Li, Y.; Xia, Y.-L.; Ai, S.-M.; Liang, J.; Sang, P.; Ji, X.-L.; Liu, S.-Q. Insights into protein–ligand interactions: mechanisms, models, and methods. *Int. J. Mol. Sci.* **2016**, *17*, 144.
- (27) Chen, F.; Wang, Z.; Wang, C.; Xu, Q.; Liang, J.; Xu, X.; Yang, J.; Wang, C.; Jiang, T.; Yu, R. Application of reverse docking for target prediction of marine compounds with anti-tumor activity. *J. Mol. Graphics Modell.* **2017**, *77*, 372–377.
- (28) Faham, S.; Hileman, R. E.; Fromm, J. R.; Linhardt, R. J.; Rees, D. C. Heparin structure and interactions with basic fibroblast growth factor. *Science* **1996**, *271*, 1116–1120.
- (29) Jiang, H.; Xu, Y.; Na, L.; Jin, R.; Zhang, S. UV-vis Spectral Analysis of Inclusion Complexes between  $\beta$ -Cyclodextrin and Aromatic/Aliphatic Guest Molecules. *Curr. Drug Discovery Technol.* **2008**, *5*, 173–176.
- (30) Cao, S.; Zhou, X.; Yang, Y.; Zhong, W.; Sun, T. Selective Substitution of 31/42-OH in Rapamycin Guided by an in Situ IR Technique. *Molecules* **2014**, *19*, 7770–7784.
- (31) Pant, A.; Negi, J. S. Novel controlled ionic gelation strategy for chitosan nanoparticles preparation using TPP- $\beta$ -CD inclusion complex. *Eur. J. Pharm. Sci.* **2018**, *112*, 180–185.
- (32) Yuan, C.; Jin, Z.; Xu, X. Inclusion complex of astaxanthin with hydroxypropyl- $\beta$ -cyclodextrin: UV, FTIR, <sup>1</sup>H NMR and molecular modeling studies. *Carbohydr. Polym.* **2012**, *89*, 492–496.
- (33) Negi, J. S.; Chattopadhyay, P.; Sharma, A. K.; Ram, V. Preparation of gamma cyclodextrin stabilized solid lipid nanoparticles (SLNS) using stearic acid- $\gamma$ -cyclodextrin inclusion complex. *J. Inclusion Phenom. Macrocyclic Chem.* **2014**, *80*, 359–368.
- (34) Xu, F.; Yang, Q.; Wu, L.; Qi, R.; Wu, Y.; Li, Y.; Tang, L.; Guo, D.; Liu, B. Investigation of inclusion complex of patchouli alcohol with  $\beta$ -cyclodextrin. *PLoS One* **2017**, *12*, No. e0169578.
- (35) Fahr, A. Cyclosporin clinical pharmacokinetics. *Clin. Pharmacokinet.* **1993**, *24*, 472–495.
- (36) Hu, C.; Yin, W.-j.; Li, D.-y.; Ding, J.-j.; Zhou, L.-y.; Wang, J.-l.; Ma, R.-r.; Liu, K.; Zhou, G.; Zuo, X.-c. Evaluating tacrolimus pharmacokinetic models in adult renal transplant recipients with different CYP3A5 genotypes. *Eur. J. Clin. Pharmacol.* **2018**, *74*, 1437–1447.
- (37) Wachter, V. J.; Salphati, L.; Benet, L. Z. Active secretion and enterocytic drug metabolism barriers to drug absorption. *Adv. Drug Delivery Rev.* **2001**, *46*, 89–102.
- (38) Lamoureux, F.; Picard, N.; Boussera, B.; Sauvage, F.-L.; Marquet, P. Sirolimus and everolimus intestinal absorption and interaction with calcineurin inhibitors: a differential effect between cyclosporine and tacrolimus. *Fundam. Clin. Pharmacol.* **2012**, *26*, 463–472.
- (39) Yunomae, K.; Arima, H.; Hirayama, F.; Uekama, K. Involvement of cholesterol in the inhibitory effect of dimethyl- $\beta$ -

cyclodextrin on P-glycoprotein and MRP2 function in Caco-2 cells. *FEBS Lett.* **2003**, *536*, 225–231.

(40) Cai, C.; Zhu, H.; Chen, J. Overexpression of caveolin-1 increases plasma membrane fluidity and reduces P-glycoprotein function in Hs578T/Dox. *Biochem. Biophys. Res. Commun.* **2004**, *320*, 868–874.

(41) Shing, Y.; Folkman, J.; Weisz, P. B.; Joullie, M. M.; Ewing, W. R. Affinity of fibroblast growth factors for  $\beta$ -cyclodextrin tetradecasulfate. *Anal. Biochem.* **1990**, *185*, 108–111.

(42) Hsu, Y.-R.; Nybo, R.; Sullivan, J. K.; Costigan, V.; Spahr, C. S.; Wong, C.; Jones, M.; Pentzer, A. G.; Crouse, J. A.; Pacifici, R. E.; Lu, H. S.; Morris, C. F.; Philo, J. S. Heparin Is Essential for a Single Keratinocyte Growth Factor Molecule To Bind and Form a Complex with Two Molecules of the Extracellular Domain of Its Receptor. *Biochemistry* **1999**, *38*, 2523–2534.

(43) Spivak-Kroizman, T.; Lemmon, M. A.; Dikic, I.; Ladbury, J. E.; Pinchasi, D.; Huang, J.; Jaye, M.; Crumley, G.; Schlessinger, J.; Lax, I. Heparin-induced oligomerization of FGF molecules is responsible for FGF receptor dimerization, activation, and cell proliferation. *Cell* **1994**, *79*, 1015–1024.

(44) Zhang, F.; Zhang, S.; Pollack, S. F.; Li, R.; Gonzalez, A. M.; Fan, J.; Zou, J.; Leininger, S. E.; Pavia-Sanders, A.; Johnson, R.; Nelson, L. D.; Raymond, J. E.; Elsbahy, M.; Hughes, D. M. P.; Lenox, M. W.; Gustafson, T. P.; Wooley, K. L. Improving paclitaxel delivery: in vitro and in vivo characterization of PEGylated polyphosphoester-based nanocarriers. *J. Am. Chem. Soc.* **2015**, *137*, 2056–2066.

(45) Chen, G.; Jiang, M. Cyclodextrin-based inclusion complexation bridging supramolecular chemistry and macromolecular self-assembly. *Chem. Soc. Rev.* **2011**, *40*, 2254–2266.

(46) Gao, S.; Sun, J.; Fu, D.; Zhao, H.; Lan, M.; Gao, F. Preparation, characterization and pharmacokinetic studies of tacrolimus-dimethyl- $\beta$ -cyclodextrin inclusion complex-loaded albumin nanoparticles. *Int. J. Pharm.* **2012**, *427*, 410–416.

(47) Chen, Y.; Huang, Y.; Qin, D.; Liu, W.; Song, C.; Lou, K.; Wang, W.; Gao, F.  $\beta$ -cyclodextrin-based inclusion complexation bridged biodegradable self-assembly macromolecular micelle for the delivery of paclitaxel. *PLoS One* **2016**, *11*, No. e0150877.

(48) Varan, G.; Patrulea, V.; Borchard, G.; Bilensoy, E. Cellular Interaction and Tumoral Penetration Properties of Cyclodextrin Nanoparticles on 3D Breast Tumor Model. *Nanomaterials* **2018**, *8*, 67.

(49) Gfeller, D.; Michielin, O.; Zoete, V. Shaping the interaction landscape of bioactive molecules. *Bioinformatics* **2013**, *29*, 3073–3079.

(50) Trott, O.; Olson, A. J. AutoDock Vina: improving the speed and accuracy of docking with a new scoring function, efficient optimization and multithreading. *J. Comput. Chem.* **2010**, *30*, 455–461.

(51) Duhovny, D.; Nussinov, R.; Wolfson, H. J. In Efficient Unbound Docking of Rigid Molecules, *International workshop on algorithms in bioinformatics*; Springer: 2002; pp 185–200.

(52) Schneidman-Duhovny, D.; Inbar, Y.; Nussinov, R.; Wolfson, H. J. PatchDock and SymmDock: servers for rigid and symmetric docking. *Nucleic Acids Res.* **2005**, *33*, W363–W367.

(53) Everolimus PubChem Compound Database, <https://pubchem.ncbi.nlm.nih.gov/compound/Everolimus>.

(54)  $\beta$ -cyclodextrin PubChem Compound Database, <https://pubchem.ncbi.nlm.nih.gov/compound/beta-CYCLODEXTRIN>.

(55) Ferreira, L. G.; Dos Santos, R. N.; Oliva, G.; Andricopulo, A. D. Molecular docking and structure-based drug design strategies. *Molecules* **2015**, *20*, 13384–13421.

(56) El-Nakkady, S. S.; Hanna, M. M.; Roaiah, H. M.; Ghannam, I. A. Y. Synthesis, molecular docking study and antitumor activity of novel 2-phenylindole derivatives. *Eur. J. Med. Chem.* **2012**, *47*, 387–398.

(57) Wallace, A. C.; Laskowski, R. A.; Thornton, J. M. LIGPLOT: a program to generate schematic diagrams of protein-ligand interactions. *Protein Eng.* **1995**, *8*, 127–134.

(58) Laskowski, R. A.; Swindells, M. B. LigPlot+: multiple ligand-protein interaction diagrams for drug discovery. *J. Chem. Inf. Model.* **2011**, *51*, 2778–2786.

(59) Miecznik, P.; Kaczmarek, M. Ultrasonic investigations of inclusion complexation of  $\alpha$ -cyclodextrin by iodide ions in pseudo-binary aqueous system. *J. Mol. Liq.* **2007**, *133*, 120–124.

(60) Chen, W.; Yang, L.-J.; Ma, S.-X.; Yang, X.-D.; Fan, B.-M.; Lin, J. Crassicauline A/ $\beta$ -cyclodextrin host-guest system: Preparation, characterization, inclusion mode, solubilization and stability. *Carbohydr. Polym.* **2011**, *84*, 1321–1328.

(61) Bird, C.; Kirstein, S. Real-time, label-free monitoring of cellular invasion and migration with the xCELLigence system. *Nat. Methods* **2009**, *6*, 622.

(62) Chiu, C.-H.; Lei, K. F.; Yeh, W.-L.; Chen, P.; Chan, Y.-S.; Hsu, K.-Y.; Chen, A. C.-Y. Comparison between xCELLigence biosensor technology and conventional cell culture system for real-time monitoring human tenocytes proliferation and drugs cytotoxicity screening. *J. Orthop. Surg. Res.* **2017**, *12*, 149.

(63) Kadletz, L.; Heiduschka, G.; Domayer, J.; Schmid, R.; Enzenhofer, E.; Thurnher, D. Evaluation of spheroid head and neck squamous cell carcinoma cell models in comparison to monolayer cultures. *Oncol. Lett.* **2015**, *10*, 1281–1286.

(64) Horning, J. L.; Sahoo, S. K.; Vijayaraghavalu, S.; Dimitrijevic, S.; Vasir, J. K.; Jain, T. K.; Panda, A. K.; Labhasetwar, V. 3-D tumor model for in vitro evaluation of anticancer drugs. *Mol. Pharmaceutics* **2008**, *5*, 849–862.